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The clinical impact of glenoid concavity and version on anterior shoulder stability

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1 **The clinical impact of glenoid concavity and version on anterior shoulder stability**

2 **Short title: Glenoid concavity & version in shoulder instability**

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1 **The clinical impact of glenoid concavity and version on anterior shoulder stability**

2 **Background:**

3 In recent biomechanical studies, the importance of glenoid concavity and version for anterior
4 shoulder stability has been highlighted. With this study, we aimed at assessing their clinical
5 relevance as stabilizing factors. We hypothesized that low glenoid concavity and low
6 retroversion are associated with anterior glenohumeral instability.

7 **Methods:**

8 In this single-center, retrospective case-control study, CT scans of n=34 patients following acute
9 anteroinferior glenohumeral dislocation between 2015 and 2021 were included. Patients with
10 glenoid fractures and preexisting glenohumeral pathologies were excluded. In the control
11 group, n=68 polytrauma patients referred to our level-I-trauma center were included, who
12 neither showed acute nor chronic glenohumeral pathologies. Both groups were matched age-
13 and gender-specifically in a 2:1 ratio.

14 Glenoid concavity was measured according to the BSSR in anterior-posterior (a.p.) and
15 superior-inferior (s.i.) direction. Version was measured by the glenoid vault method.

16 **Results:**

17 The instability cohort presented with a lower BSSR(s.i.) compared to the control group (49.8%
18 vs. 56.9%, p=0.001). The BSSR(a.p.) did not differ significantly (30.2% vs. 33.7%, p=0.163).

19 A higher retroversion was seen in the instability cohort (-13.1° vs. -11.4°; p=0.041). Subgroup
20 analyses showed higher BSSR(s.i.) in ≥60-year-old patients compared to ≤30-year-old patients.

21 BSSR(a.p.) and glenoid version did neither differ age- nor gender-specifically.

22 **Conclusion:**

23 Glenoid concavity is a relevant factor for anterior shoulder stability in the clinical setting. In
24 contrast to recent biomechanical studies, glenoid version appears to have only limited clinical

25 impact on anterior stability. Regarding the individual treatment of anterior glenohumeral
26 instability, glenoid concavity should be focused on as an essential bony stabilizing factor.

27 **Keywords:** Glenoid concavity, BSSR, glenoid version, anterior shoulder instability, shoulder
28 joint dislocation

29 **Level of evidence:** Level III; Retrospective Case-Control Design; Prognosis Study

30 The understanding of shoulder stability has become more differentiated throughout the last
31 years and glenoid concavity as well as glenoid version have been investigated in recent studies.
32 Still, the clinical relevance of glenoid concavity and version as bony stabilizing factors in the
33 context of anterior shoulder stability is unknown, yet.

34 The principle of concavity-compression describes the synergy of both, the glenoid concavity
35 and the rotator cuff's compressive force, centering the humeral head within the glenoid and
36 therefore providing glenohumeral stability^{7,15,16}. Regarding glenoid concavity, recent
37 biomechanical studies include finite elements analyses, bony glenohumeral models as well as
38 active-assisted shoulder models, considering the concavity-compression mechanism^{20,21,23,30}.

39 Here it has been shown that the glenoid concavity is an essential factor for anterior shoulder
40 stability, and instability is mainly caused by the loss of concavity³⁰. Highly concave-shaped
41 glenoids were shown to tolerate up to 20% glenoid bone loss, until stability was reduced to the
42 level of native joints with low concavity²³. Moroder et al established the computed tomography
43 (CT) based bony shoulder stability ratio (BSSR), describing the glenoid concavity considering
44 the glenoid radius and depth²¹. However, the role of the glenoid concavity in a clinical setting
45 and physiological ranges of concavity are yet unknown.

46 Regarding the glenoid version, a mild retroversion can be observed in physiological conditions.
47 In the following, 0° equals a neutral glenoid version, while positive and negative numeric values
48 describe anteversion and retroversion, respectively. The most common methods of measuring
49 glenoid version include the Friedman method and the glenoid vault method. According to

50 Friedman et al, a line is drawn from the most medial point of the scapula to the center of a line
51 connecting the anterior and posterior glenoid rim⁴. According to Matsumura et al describing the
52 glenoid vault method, a line connecting the tip of the triangular-shaped glenoid vault and the
53 center of the glenoid articular surface is used for measuring glenoid version. Thus, the
54 individual morphology of the scapula body cannot confound the measurement¹⁷. For the glenoid
55 vault method, physiological ranges of $-8.9^{\circ} (\pm 2.7^{\circ})^{17}$ and $-8^{\circ} (\pm 4.9^{\circ})^2$ retroversion are described
56 in literature. Regarding the Friedman method, smaller numeric values are described with a
57 physiological range of $-2.1^{\circ} (\pm 4.7^{\circ})^2$.

58 Biomechanically, Eichinger et al could show that the glenoid version influences both, anterior
59 and posterior shoulder stability in a linear correlation. In their model, every 1° increase of
60 anteversion led to a 6% decrease of anteroinferior dislocation force³. Also, the humeral head
61 position is influenced by glenoid version, as Imhoff et al pointed out. With every 5° increase of
62 retroversion, the humeral head was positioned about 2 mm more posteriorly within the glenoid
63 cavity⁹.

64 Clinically, a correlation between increased retroversion and posterior shoulder instability is
65 described in several studies^{5,6,11,12,18,24,26,28}. Regarding anterior shoulder stability, however, the
66 clinical impact of glenoid version is not as clear. Only few studies have yet analyzed patient
67 cohorts with anterior instability. In some of these studies, anterior instability collectives were
68 associated with a slightly decreased retroversion, compared to control cohorts without shoulder
69 instability^{1,8}. However, glenoid version in the instability groups did not clearly exceed
70 physiological ranges. Furthermore, Privitera et al found no significant difference in glenoid
71 version between asymptomatic and anteriorly unstable patients²⁸. Thus, the clinical relevance
72 of glenoid version in the context of anterior shoulder stability yet remains unclear.

73 In this study, the clinical impact of glenoid concavity and glenoid version on anterior shoulder
74 stability were analyzed. Comparing patients with anterior instability to a control cohort without

75 shoulder instability, we hypothesized that anterior instability is associated with lower glenoid
76 concavity and less glenoid retroversion.

77 **Materials and Methods:**

78 **Study design**

79 This retrospective case-control study was performed at the Department of Trauma, Hand and
80 Reconstructive Surgery of the University Hospital Münster, Germany, a level-1-trauma center,
81 and approved by the institutional review board (IRB No. 2021-607-f-S, University of Münster,
82 Germany). CT scans of patients presenting with an acute, anteroinferior shoulder joint
83 dislocation between 2015 and 2021 were evaluated and compared to a control cohort. Exclusion
84 criteria included glenoid fractures, incomplete glenoid imaging in the CT scan, previous
85 episodes of shoulder joint dislocation, multidirectional shoulder instability and preexisting
86 shoulder joint pathologies. Patient data were obtained via the hospital's documentation system
87 Orbis (Dedalus, Bonn, Germany) and n=34 patients were included in the instability cohort.
88 Detailed numbers of patients after applying inclusion and exclusion criteria are presented in
89 figure 1.

90 The control cohort was comprised of polytraumatized patients admitted to our hospital from
91 January 2020 to October 2021, receiving polytrauma CT scans, including glenohumeral joint
92 imaging. Patients without acute and chronic glenohumeral pathologies were included in the
93 control collective. A gender and age dependent matching in a 2:1 ratio was performed between
94 instability and control cohort, resulting in n=68 patients within the control group. Specifically,
95 for every patient within the instability cohort, two same-gender patients were matched, in which
96 the equal-sided shoulder was analyzed. Age-specific matching was performed as precise as

97 possible. For n=20 instability patients, two control patients of ± 2 years of age were matched.

98 The maximum age difference within the remaining matched patients was six years.

99 In addition, subgroups were formed in order to examine the influence of gender (female vs.

100 male) and age (≤ 30 vs. ≥ 60 years of age) on glenoid concavity and version.

101 **Measurements:**

102 Radiological measurements were acquired with Aquarius iNtuition (version 4.4, TeraRecon,

103 Durham, NC, USA) using individual multiplanar reconstruction of the CT scan data. CT scan

104 thickness was 1-1.5mm.

105 Joint-specific coordinate systems were established by creating superior-inferior (s.i.) and

106 anterior-posterior (a.p.) axes aligned to the most superior, inferior, anterior and posterior points

107 of the glenoid rim, respectively. The mediolateral axis was added orthogonally to both, the s.i.

108 and a.p. axes.

109 Glenoid concavity was measured according to the CT-based BSSR including glenoid radius (r)

110 and depth (d)²¹.

$$111 \quad BSSR = \frac{1 - \left(\frac{r-d}{r}\right)^2}{\frac{r-d}{r}}$$

112 Measurement of the BSSR were performed in both, coronal and axial planes, so that the

113 superior-inferior concavity (BSSR(s.i.)) and anterior-posterior concavity (BSSR(a.p.)) were

114 analyzed, respectively. The glenoid radius was measured using the best-fit-circle method as

115 described by Kuberakani et al¹⁴ (see figure 2). The glenoid depth (d) was measured by defining

116 the widest s.i. and a.p. glenoid diameter, which equal the s.i. and a.p. axes, respectively.

117 Orthogonally to each axis, the maximum glenoid depth was measured at each axis' center point

118 in both, coronal and axial planes (see figure 2).

119 The measurement of glenoid version was based on the glenoid vault method as described by
120 Matsumura et al.¹⁷ While Matsumura et al aligned the planes of CT scans to the individual
121 scapula body, in this study the previously described coordinate system aligned to the glenoid
122 was used. Except different CT plane alignments, the measurement of glenoid version was
123 performed analogously to Matsumura et al. In an axial plane a line was then drawn connecting
124 the tip of the triangle-shaped glenoid vault and the center of the glenoid articular surface. A
125 perpendicular line indicated 0° of glenoid version and was then used for measuring the
126 individual, patient-specific version (see figure 3).

127 **Statistical Analysis:**

128 An *a priori* power analysis using G*Power (version 3.1.9.7; Heinrich Heine Universität,
129 Düsseldorf, Germany) was performed to determine the necessary sample size. Here, the mean
130 BSSR(a.p.) values of the cadaveric study of Wermers et al were used and compared to five
131 BSSR(a.p.) test measurements within the instability cohort of this study. With an alpha level of
132 0.05, a power of 0.95 and an effect size of $d=0.942$, required numbers of patients for unpaired
133 t-tests were calculated. Here, numbers of $n=23$ patients for the instability cohort, and $n=45$
134 patients for the control group were defined.

135 Statistics were performed using GraphPad Prism® (GraphPad Software Inc., San Diego, CA,
136 USA). Descriptive statistics including median and mean values, standard deviation, range, as
137 well as 25th and 75th percentiles were calculated for all variables. Normal distribution was
138 assessed graphically via quantile-quantile-plot (QQ-Plot) as well as the Shapiro-Wilk-test.

139 A level of $p<0.05$ was deemed significant. For group comparisons, the t-test was used. For
140 parameters not showing normal distribution, the Mann-Whitney-U-Test was applied,
141 additionally. This was performed for both, comparing instability and control cohort, as well as
142 analyzing age- and gender-specific subgroups. Correlation between different parameters was

143 tested using a linear regression model. Binary logistic regression was used to analyze the impact
144 of concavity on the occurrence of shoulder instability, presented with Odds ratios (OR) and the
145 OR's 95% confidence intervals (CI). A post-hoc power analysis was performed to verify the
146 preliminarily set confidence interval of 95%.

147 **Results:**

148 **Study population:**

149 In the instability cohort, n=34 patients were included, while the control cohort consists of n=68
150 patients after matching. Throughout all included patients, the mean age was 48 years (± 19.9 ;
151 18 – 92). Within instability and control cohort, the patients' mean age was 46.9 (± 20.3) and
152 48.6 (± 19.9) years, respectively. Within each group, 26.5% of patients were female, 73.5% were
153 male. Within the instability cohort, n=19 patients presented with a right shoulder injury, while
154 in n=15 patients the left shoulder was affected. Regarding the mechanism of injury within the
155 instability cohort, two patients presented with atraumatic shoulder dislocations and hyperlaxity.
156 Five patients sustained dislocations after seizures, while the remaining n=27 patients described
157 adequate trauma (falling, sports injuries, vehicle/traffic accidents). A spontaneous
158 glenohumeral reposition was observed in three patients, while n=31 patients required closed
159 reduction.

160 **Primary Outcome:**

161 Glenoid concavity and version were measured and compared between instability and control
162 cohort (see figure 4). The mean BSSR(s.i.) in the instability group was 49.8% (± 9.0), while the
163 control cohort showed a mean BSSR(s.i.) of 56.9% (± 9.9). Therefore, patients in the instability
164 cohort presented with a significantly lower concavity in the superior-inferior axis compared to

165 the control group ($p=0.0007$). Regarding the glenoid concavity in the anterior-posterior axis,
166 the difference between instability and control group showed no statistical significance
167 ($p=0.1634$). Here, the instability group showed a mean BSSR(a.p.) of 30.15% (± 13.63), while
168 the control group presented with a BSSR(a.p.) of 33.72% (± 11.44). Details are described in
169 table 1.

170 Binary logistic regression analyses showed that with every 1% increase in BSSR(s.i.), the risk
171 of anteroinferior shoulder instability decreases by 8% (OR 0.92; 95% CI 0.87 – 0.97;
172 $p=0.0017$). Regarding a 1% increase of the BSSR(a.p.), the decreased risk of shoulder
173 instability was not significant (OR 0.98; 95% CI 0.94 – 1.01; $p=0.1695$).

174 In the overall study population, BSSR(s.i.) and BSSR(a.p.) showed a low correlation with a
175 determination coefficient of $R^2=0.23$ in a linear regression model.

176 For evaluation of the BSSR, glenoid radius and depth were assessed in both, axial and coronal
177 planes. Radius and depth were analyzed separately to detect specific differences, masked by the
178 BSSR. Here, the instability group presented with a significantly higher glenoid radius in both
179 planes. Regarding glenoid depth in coronal planes, significantly higher values were seen in the
180 control group compared to patients in the instability cohort ($p=0.0115$), while in axial planes
181 the glenoid depth did not differ significantly ($p=0.5974$). These results are consistent with the
182 BSSR providing significant differences only in coronal planes. Details are shown in table 1.

183 Assessment of glenoid version showed more retroversion in the instability cohort with a mean
184 glenoid version angle of -13.14° (± 4.38 ; -22.6 – -5). In the control group a mean glenoid version
185 of -11.44° (± 3.66 ; -18.7 – -3.3) was seen, showing significantly less retroversion ($p=0.0407$).

186 In the linear regression model, the glenoid version did not correlate with BSSR(s.i.) and
187 BSSR(a.p.) with determination coefficients of $R^2=0.0144$ and $R^2=0.0016$, respectively.

188 **Subgroup analyses:**

189 Within the instability and control cohorts, age and gender-specific subgroups were defined (see
190 figures 5a/b, 6).

191 To evaluate age-dependent differences in concavity and version and their impact on shoulder
192 stability, patients ≤ 30 years of age were compared to patients ≥ 60 years of age (see figure 5a).
193 Regarding the BSSR(a.p.), no significant differences were seen between ≤ 30 and ≥ 60 -year-old
194 patients within both, instability and control cohort ($p=0.4409$; $p=0.19$, respectively). In contrast,
195 ≤ 30 -year-old patients showed a lower mean BSSR(s.i.) than ≥ 60 -year-old patients within the
196 instability cohort (44.75% (± 9.02) vs. 56.11% (± 8.98), $p=0.0218$). While a significantly lower
197 BSSR(s.i.) in the instability cohort compared to the control group was evident in ≤ 30 -year-old
198 patients (44.75% (± 9.02) vs. 56.33% (± 9.73), $p=0.0064$), in ≥ 60 -year-old patients, no difference
199 was seen between instability and control cohort (56.11% (± 8.98) vs. 62.4% (± 10.12),
200 $p=0.1647$). Within the control group, BSSR(s.i.) differences between ≤ 30 and ≥ 60 -year-old
201 patients were not significant ($p=0.091$). Regarding glenoid version, no age-specific differences
202 were found ($p \geq 0.347$) (see figure 6).

203 Comparing female to male patients within each cohort, no significant differences were seen
204 regarding BSSR(a.p.) ($p \geq 0.1157$) and BSSR(s.i.) ($p \geq 0.8273$) (see figure 5b). Also, glenoid
205 version did not show gender-dependent differences within instability cohort (female -11.24°
206 (± 5.1) vs. male -13.82° (± 3.99), $p=0.1326$) and control cohort (female -11.08° (± 3.59) vs. male
207 -11.56° (± 3.51), $p=0.6321$).

208 **Discussion:**

209 In this study evaluating the clinical relevance of glenoid concavity and version for anterior
210 shoulder instability, we can summarize the following main findings: (1) Anterior shoulder
211 instability is associated with a lower glenoid concavity in coronal planes. In axial planes, the
212 same tendencies were seen, however, without showing statistical significance. (2) The role of

213 glenoid version in the context of anterior glenohumeral stability remains controversial, since in
214 this study a higher retroversion was seen in the instability cohort compared to the control group.
215 Regarding glenoid concavity, the results of this study fall in line with previous biomechanical
216 studies. Moroder et al described the stabilizing effect of glenoid concavity by finite element
217 analysis. In case of osseous Bankart lesions, they suggested that the loss of concavity might be
218 a more precise parameter indicating anterior glenohumeral instability than conventional, two-
219 dimensional methods measuring the glenoid defect size^{20,21}. Previous biomechanical results of
220 our working group confirmed the importance of glenoid concavity. In an osteochondral model
221 using cadaveric glenoids and humeral heads, a high correlation between concavity and stability
222 was found, while the loss of concavity served as a precise predictor for anterior shoulder
223 instability³⁰. This was confirmed in an active-assisted cadaveric model including soft tissue and
224 the rotator cuff's compressive forces, resembling the physiological, stabilizing mechanism of
225 concavity compression^{16,23}.

226 This study underlines the importance of glenoid concavity in a clinical setting. Superior-inferior
227 concavity was lower in the instability cohort. The same tendency of lower a.p. concavity was
228 found in the instability group and the difference might become significant with a larger study
229 population. One could also suggest, that inferior glenoid concavity plays a more important role
230 in preventing anteroinferior glenohumeral dislocation than anterior concavity. This could be
231 explained by other, mainly anteriorly located, anatomical structures like the coracoid or the
232 conjoint tendons, as well as individual labral morphology and anterior capsular tension, helping
233 to prevent anterior humeral head translation. However, further biomechanical studies are
234 required to draw final conclusions to this assumption. The specific anteroinferior concavity
235 within the track of humeral head dislocation as well as the correlation of glenoid concavity,
236 version and inclination should be included.

237 Regarding glenoid version in the context of anterior shoulder stability, the results in this study
238 do not support the findings of previous biomechanical and clinical studies. Biomechanically,
239 Eichinger et al found a linear correlation between glenoid version and both, anterior and
240 posterior stability with increased anteversion causing anterior instability and vice versa³. Imhoff
241 et al described a more posterior humeral head position in case of increased glenoid retroversion,
242 leading to increased posterior instability⁹. While the association of increased glenoid
243 retroversion and posterior glenohumeral instability became apparent in several clinical
244 studies^{5,6,12,24,26,28}, the clinical correlation of glenoid anteversion and anterior stability remains
245 ambiguous. Only few studies compared a cohort with anterior instability to patients without
246 shoulder instability. Privitera et al did not find a significant difference in glenoid version
247 between both groups²⁸. Hohmann et al and Aygün et al describe a slightly higher anteversion in
248 anterior instability cohorts, however, the amount of glenoid version barely exceeds
249 physiological ranges^{2,17}. In this study, the anterior instability cohort controversially presented
250 with higher retroversion compared to the control cohort, leading to the assumption that glenoid
251 version provides only limited influence on anterior glenohumeral stability.

252 Another possible explanation for the presented results could be a reciprocal, anatomical
253 adaption of glenoid version and concavity. For example, an increased glenoid retroversion
254 would counteract a low native concavity, reducing anterior instability. However, a low
255 correlation between glenoid concavity and version in this study does not support this theory.
256 Still, we consider the relation between concavity and version to be worth analyzing in larger,
257 differentiated patient cohorts to produce more detailed results.

258 In subgroup analyses, it was evident that especially in coronal planes, older patients presented
259 with a higher glenoid concavity. We consider this finding to be mainly caused by degenerative
260 changes leading to increased, central glenoid depth and, therefore, increased concavity^{10,29}. It
261 was striking that in ≥ 60 -year-old patients, axial and coronal glenoid concavity did not differ

262 between instability and control cohort. This leads to the suggestion that concavity only plays a
263 minor role in older patients, while low concavity in young patients was evidently associated
264 with anterior shoulder instability. Regarding gender-specific analyses, no relevant differences
265 were seen. Glenoid version did neither show age- nor gender-specific differences.

266 Limitations of this study include the retrospective study design. A higher number of patients
267 included in this study would have been desirable, however, the required study population
268 according to the power analysis was exceeded. The higher mean age of the instability cohort
269 compared to larger shoulder dislocation cohorts^{13,22,25} must be mentioned, as well. A reason for
270 this could be the fact that younger patients were shown to have a higher risk of sustaining
271 Bankart fractures¹⁹, making them not eligible for inclusion. Also, a relevant number of
272 especially younger patients suffering from anteroinferior shoulder dislocation without glenoid
273 bone loss could not be included, due to reasonable diagnostic algorithms. Especially in younger
274 patients, magnetic resonance imaging (MRI) is preferred over CT scans in the absence of signs
275 for bony glenoid injury in the initial X-ray images.

276 Another factor limiting the accuracy of the results is the comparably high slice thickness of 1 –
277 1.5 mm of the polytrauma CT scans, which were performed in an emergency setting and
278 retrospectively used to generate the control cohort. Minimal changes in concavity and version
279 can significantly alter the measurements and, therefore, thinner CT scan slices would have
280 increased the validity of this study. Also, possible degenerative, cartilage lesions, especially in
281 older patients, as well as individual labral morphology were not detected by CT scans.

282 The method of measuring glenoid version has to be mentioned as a possible limitation, as well.
283 The most commonly used techniques include the Friedman method as well as glenoid vault
284 methods^{4,17,27}. Since the polytrauma CT scans of the control cohort do not regularly include the
285 most medial aspects of the scapula body, the Friedman method could not be applied in this
286 study. Also, the glenoid vault method according to Matsumura had to be adjusted, since

287 originally the entire scapula body is necessary for CT plane alignment¹⁷. In this study, the
288 coordinate system aligned to the glenoid surface in order to measure concavity was also used
289 for assessing glenoid version. This slight CT plane deviation might explain that previously
290 published ranges of retroversion are exceeded in both, instability and control cohort of this
291 study. Still, we assume that the comparison of version between both cohorts and the correlation
292 between version and concavity within this study remains reliable.

293 Future studies including a higher number of patients and high-quality CT imaging should be
294 performed to confirm the clinical relevance of the glenoid concavity in both, native joints and
295 in the presence of glenoid bone loss. Also, the yet controversial role of glenoid version in the
296 context of anterior shoulder stability should be addressed. Furthermore, MRI scan evaluation
297 could include the morphology of glenoid cartilage and labrum, resulting in individual
298 glenolabral concavity and version.

299 **Conclusion:**

300 Glenoid concavity is a relevant factor for anterior shoulder stability, not only in biomechanical
301 models but also in a clinical setting.

302 The role of glenoid version remains controversial, since in this study it appears to have only
303 limited clinical impact on anterior stability.

304 In an individual therapeutic approach on anterior glenohumeral instability, glenoid concavity
305 should be focused on as an essential bony stabilizing factor.

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409 **Figure 1)** Flow diagram showing the number of patients eligible and included in this study after
410 applying inclusion and exclusion criteria.

411 **Figure 2)** Measurement of the glenoid radius with the best-fit-circle method (a, b) and the
412 glenoid depth (c, d). Both were measured in axial (a, c) and coronal (b, d) planes.

413 **Figure 3)** Measurement of the glenoid version based on the glenoid vault method, described by
414 Matsumura et al.

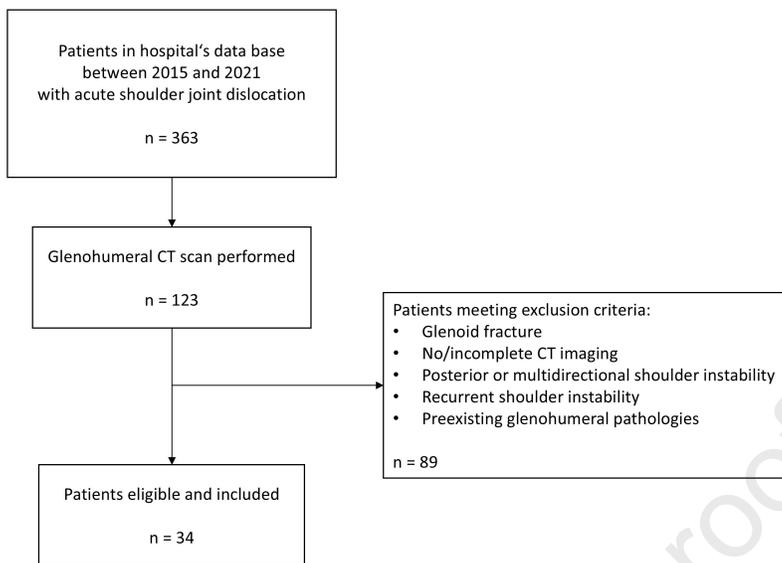
415 **Figure 4)** Boxplots and analyses of glenoid concavity (a) and version (b) between instability
416 cohort (dark blue) and control cohort (light blue).

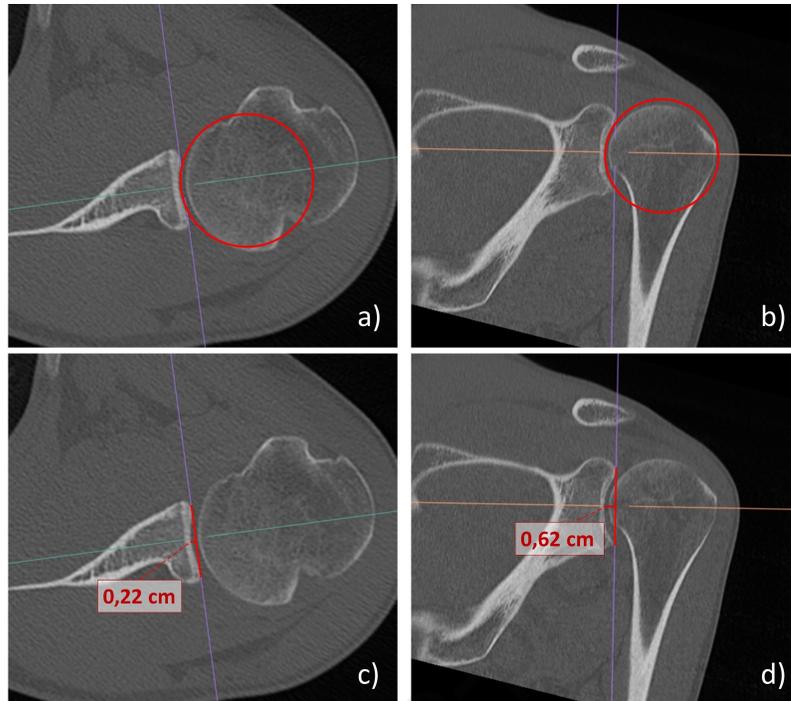
417 **Figure 5)** Age-specific (a) and gender-specific (b) subgroup analyses of the glenoid concavity
418 in axial planes (a.p., blue) and coronal planes (s.i., green) are shown. Patients were compared
419 regarding (a) age (≤ 30 years old vs. ≥ 60 years old) and (b) gender (female vs. male).

420 **Figure 6)** Age-specific and gender-specific subgroup analyses of the glenoid version. Patients
421 were compared regarding age (≤ 30 years old vs. ≥ 60 years old) and gender (female vs. male).

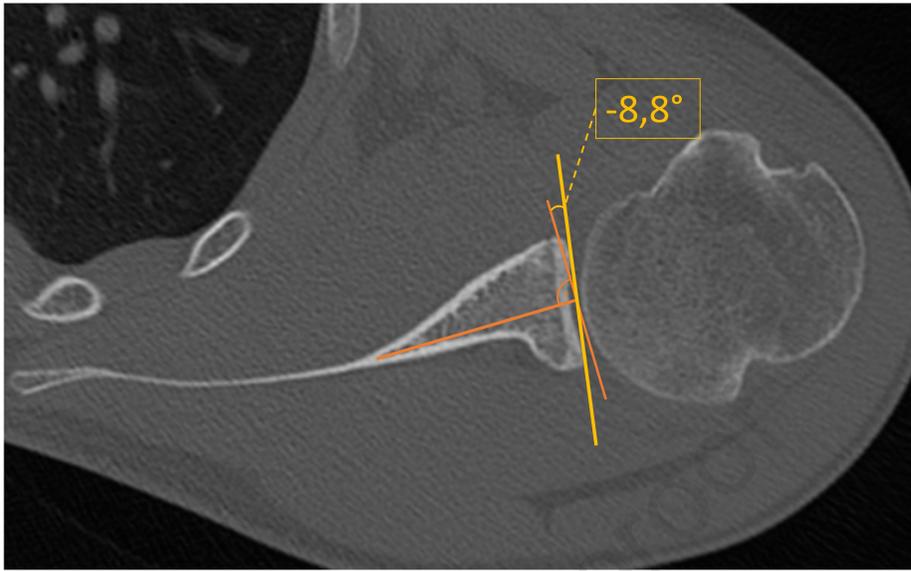
422 **Table 1)** Detailed values (mean, standard error of mean, range) and statistical analyses of
423 glenoid radius, depth, the bony shoulder stability ratio (BSSR) and glenoid version. Radius,
424 depth and BSSR were assessed in coronal planes in a superior-inferior (s.i.) axis, as well as in
425 axial planes in an anterior-posterior (a.p.) axis. Statistical analysis was either performed by t-
426 tests ^(a) or Mann-Whitney-U-Tests ^(b) depending on the distribution of values.

	Instability cohort	Control cohort	p-value
Glenoid radius (coronal)	36.54 (± 7.8 ; 22.8 – 64)	32.59 (± 4.91 ; 23,4 – 50.5)	0.0048 ^(b)
Glenoid radius (axial)	43.72 (± 14.81 ; 19.25 – 81)	36.58 (± 8.2 ; 22.65 – 61)	0.0241 ^(b)
Glenoid depth (coronal)	3.72 (± 0.79 ; 1.9 – 5.36)	4.18 (± 0.88 ; 2.03 – 6.2)	0.0115 ^(a)
Glenoid depth (axial)	1.73 (± 0.85 ; 0 – 3.42)	1.89 (± 0.89 ; 0.01 – 4.95)	0.5974 ^(b)
BSSR (s.i./coronal)	49.82 (± 9.09 ; 31.95 – 66.42)	56.93 (± 9.94 ; 29.62 – 81.28)	0.0007 ^(a)
BSSR (a.p./axial)	30.15 (± 13.63 ; 0 – 69.19)	33.72 (± 11.44 ; 1.81 – 68.57)	0.1634 ^(b)
Glenoid version	-13.14 (± 4.38 ; -22.6 – -5)	-11.44 (± 3.66 ; -18.7 – -3.3)	0.0407 ^(a)



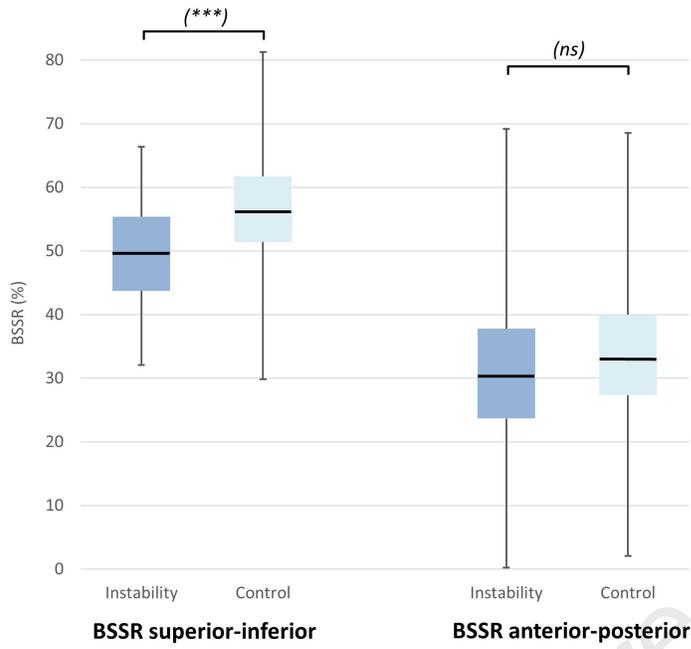


Journal Pre



Journal Pre-proof

a) Glenoid concavity



b) Glenoid version

